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European Patent Office
Office européen des brevets

Publication number:

0 362 611
A1

EUROPEAN PATENT APPLICATION

Application number: 89117237.1

Int. Cl.⁵: A61N 1/08 , A61N 1/362 ,
A61F 2/48 , H04R 25/00

Date of filing: 18.09.89

Priority: 19.09.88 DE 3831809

Date of publication of application:
11.04.90 Bulletin 90/15

Designated Contracting States:
DE FR GB NL SE

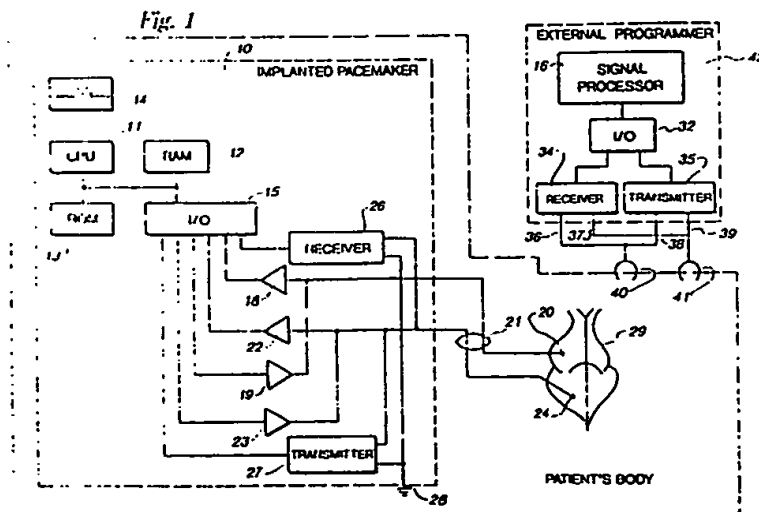
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Body bus medical device communication system.

A system intended for being at least partly implanted into a living body and comprising at least two modules or devices (10, 42) which are interconnected by a communication transmission channel, at least one of said modules (10) being provided with transmitting (27) and receiving (26) means for a bidirectional exchange of information with at least one further module and at least one other module (42) of which being provided at least with receiving means (34) or transmitting means (35) for receiving information from at least one further module or for transmitting information to at least one further module, respectively. Within the intracorporal region, said communication transmission channel is wireless. It includes the ion medium of the intra and extracellular body liquids and provides for an electrolytic-galvanic coupling between two or more implantable modules and/or between at least one implantable module (10) and external skin electrodes (40, 41) intended for connection to an external module (42). The exchange of information is effected by modulated medium frequency signals in the frequency range from 10 to 100 kHz which signals are passed through said communication transmission channel.



BODY BUS MEDICAL DEVICE COMMUNICATION SYSTEM

Background of the Invention

5 1. Field of the Invention

This invention relates to a system of medical devices intended for being at least partly implanted into a living body and comprising at least two modules which are interconnected by a communication transmission channel denoted the "body bus".

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2. Description of the Prior Art

Devices of this type are known in different embodiments, e.g. EPO 0 011 935 and EPO 0 011 936 describe an external programming device and an implantable electromedical device adapted for being 15 programmed thereby, wherein the programming device comprises a transmitting antenna, and the implantable device comprises a receiving antenna which are mutually aligned with each other for programming in order to transcutaneously transmit high frequency programming signals in the form of electromagnetic waves from the transmitting antenna to the receiving antenna. In view of the fact that high frequency 20 electromagnetic waves are heavily attenuated or screened by body tissue, the implanted receiving antenna must be exactly located for programming. Such a procedure is particularly troublesome if a plurality of programmable modules, e. g. a pacemaker, a defibrillator and a drug dispensing device, are implanted, the receiving antennas of which must be individually located.

In the case of a prior muscle stimulation apparatus (U.S. Patent 4,524,774) in a similar manner, muscle 25 potentials detected by implanted sensors are converted by a modulator into control signals for a telemetry transmitter which is integrated into the respective sensor. This telemetry transmitter transcutaneously transmits high frequency telemetry signals to an external telemetry receiver which is connected to a data processing unit. The latter, on the base of the received signals, controls a likewise externally disposed telemetry transmitter for delivering high frequency control signals, against transcutaneously, to receivers of 30 implanted muscle stimulators. The transcutaneously transmitted signals are in the megacycles/sec. frequency range so that the aforementioned restrictions are encountered in this case too.

Furthermore, it is known (Fig. 1 of U.S. Patent 4,543,955) to transmit measuring signals of an implanted sensor module through a wire connection to another implanted module, such as a pacemaker or a drug 35 delivery device. This requires, during implantation, a troublesome wiring of connection conduits. Furthermore if an infection occurs at one of the implanted modules, all modules and connection conduits must be removed because the infection can spread along the connection conduits. In conformity with modified embodiments of the last mentioned device (Figs. 2 and 5 of U.S. Patent 4,543,955) measuring signals, which have been converted into a program code, also can be unidirectionally transmitted, in a wireless 40 manner, from the sensor to the pacemaker or to the drug dispensing device, wherein either the signals defining the program code are directly transmitted through body tissue (i.e., without any carrier) or again a high frequency transmitter is used. A carrier free signal direct transmission, for being effective, must be carried through during the refractory phases, i.e. must be synchronized with the heart cycle because otherwise the signals required for such a direct transmission may provoke undesired biological reactions. On the other hand, the high frequency transmission, in this case too, poses problems because of the heavy 45 attenuation caused by body tissue and is possible, if at all, merely if the transmitting and receiving antennas are closely spaced with in the body.

SUMMARY OF THE INVENTION

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The object basic to the invention is to provide for a device of the type mentioned at the beginning which allows a signal transmission between the modules in a particularly simple, reliable and universally applicable manner while simultaneously avoiding the above discussed deficiencies.

In conformity with one aspect of the invention, this object is reached by a system intended for being at

least partly implanted into a living body and comprising at least two medical devices or modules which are interconnected by a communication transmission channel, at least one of said modules being provided with transmitting and receiving means for a bidirectional exchange of information with at least one further module and at least one other module of which being provided at least with receiving means or transmitting means
 5 for receiving information from at least one further module or for transmitting information to at least one further module, respectively, wherein within the intracorporal region said communication transmission channel is wireless, includes the ion medium of the intra and extracellular body liquids and provides for an electrolytic-galvanic coupling between two or more implantable modules and/or between at least one implantable module and external skin electrodes intended for connection to an external module and wherein
 10 the exchange of information is effected by modulated medium frequency signals in the frequency range from 10 to 100 kHz which signals are passed through said communication transmission channel by direct conduction.

According to a further aspect of the present invention a system is provided for monitoring a condition of a living body and/or providing one or more therapy regimens to the body comprising two or more discrete
 15 medical devices, at least one of which is a digitally programmable, implantable medical device and the other is an external medical device for digitally programming said implantable medical device wherein said implantable medical device is provided with:

- a pair of spaced-apart electrodes adapted to be exposed to living body tissue and fluids;
- receiving means for receiving electrical signals across said electrodes;
- 20 decoding means for decoding said electrical signals; and
- register means for storing said decoded electrical signals; and
- wherein said digital programming device further comprises:
- a pair of electrodes adapted to be placed against the external surface of the living body;
- coding means for coding a desired program change into digital code; and
- 25 transmitting means responsive to the programmed digital code for modulating said digital signal and applying it to said external pair of electrodes whereby said modulated, coded signal is applied through the skin and living body tissue to said implantable pair of electrodes.

A system for providing pacing, cardioversion and defibrillation staged therapies for bradycardia, tachycardia and fibrillation, in conformity with the present invention comprises:

- 30 a body implantable pacemaker comprising:
- a pacing energy pulse generator for applying pacing stimuli to a patient's heart;
- pacing lead means bearing at least one electrode adapted to be placed in contact with or within a patient's heart and coupled to said pulse generator means for applying said pacing stimuli to the patient's heart and receiving electrical signals appearing at the tissue-electrode interface;
- 35 sensing means coupled to said electrode means for sensing electrical signals appearing at said electrode means;
- detecting means responsive to said sensing means for detecting a bradyarrhythmia, tachyarrhythmia or ventricular fibrillation condition of the heart of the patient; and
- control means responsive to said detecting means for instructing said pulse generator means to provide
- 40 pacing stimuli to said electrodes in response to the detection of a bradyarrhythmia or tachyarrhythmia condition and in response to the detection of a ventricular fibrillation condition provide a coded instruction signal to said pulse generator means for providing electrical signals to said electrode means; and
- a remotely implanted defibrillator further comprising:
- defibrillation electrode means adapted to be placed in contact with a patient's heart for providing
- 45 defibrillation shocks to the heart and for picking up electrical signals appearing at the electrode-tissue interface;
- defibrillation pulse generator means for providing defibrillation shocks to the heart;
- receiving means coupled to said defibrillation electrodes for demodulating and decoding said coded signal transmitted into body tissue by said pacemaker pulse generator; and
- 50 means responsive to a shock instruction signal decoded by said receiving means for causing said pulse generator means to provide a shock across said defibrillation electrode and to the heart.

The present invention further provides for an implantable defibrillator-pacemaker system which is characterized in that the defibrillator is designed to have the operation thereof controlled by the separately implanted pacemaker.

55 A modulated signal in the frequency range from 10 kHz to 100 kHz has a sufficiently high frequency to not cause any polarization problems within the living body and to allow an effective filtering with high Q filters requiring only little installation space. On the other hand, this frequency range is so low that undesired high frequency phenomena, such as radiation problems, crosstalk and excessive attenuation of

the desired signals by the body tissue are avoided. Rather, modulated signals in the frequency range from 10 to 100 kHz are electrolytically-galvanically transmitted over the distances encountered in the living body with such a low attenuation that on the transmitter side signal amplitudes which biologically are certainly ineffective and which can be transmitted without any regard to the heart cycle also to electrodes which might be provided for stimulation of the heart are sufficient to allow the modulated signals to be reliably detected at the receiver side at low expenditure for filters and amplifiers.

A bidirectional exchange of information provides for an interactive mutual coupling of the individual modules. The functional interconnection between implanted and external modules may be obtained in a particularly simple manner via body fluids by making use of the electrolytical-galvanical coupling, presently also shortly named body bus, and via the skin electrodes so that a troublesome search for the antennas of the implanted module or modules is avoided.

In conformity with a further development of the invention, at least one digitally programmable implantable module and an external module in the form of a programming device are provided. The programmer would, because of the body bus bidirectional properties, enable interactive intelligent programming. Over a modem, telephone programming and control would be possible, especially a necessity for endangered tachy or defibrillator patients.

Preferred examples of implanted modules are nerve stimulators, muscle stimulators, cardiac pacemakers, defibrillators, drug dispensing devices, sensors for detecting body parameters or body activities as well as controllable and/or programmable artificial organs. Apart from the aforementioned programming devices, particularly, but not exclusively, monitoring and/or test devices may be used as external modules such as data recording devices (magnetic tape devices or the like) or models adapted for connection to telephone circuits.

If a plurality of implantable modules are provided, programming and/or intelligent decision means, in conformity with a further development of the invention, preferably are concentrated in one of the implanted modules only wherein, in case of need, other implanted modules can be indirectly programmed via said one module. Thereby it is possible to keep the hardware expenditure, the weight, the space requirements and the energy consumption of the total of implanted modules particularly small. Basically, however, it is likewise possible to provide a plurality of implanted modules comprising programming and/or intelligent decision means which modules mutually communicate via the body bus.

Preferably the modules are provided with means for receiving and/or transmitting of pulscode-modulated medium frequency signals. A1-modulated medium frequency signals may be used, i.e. the signal has a single, fixed frequency of e.g., 30 kHz, and this signal, at the transmitting side, is switched on and off as a function of the modulation. In conformity with a modified embodiment, the modules may be provided with means for receiving and/or transmitting signals which are frequency shifted between a pair of frequencies within the medium frequency range. That means a pair of predetermined fixed signal frequencies, e.g. of 30 kHz and 40 kHz are used, and shifting takes place at the transmitting side between the two signal frequencies as a function of the modulation. The pulscode modulation avoids sidebands and continuous frequency swings. The one or the two signal frequencies can be generated at the transmitting side by means of crystal oscillators with a high frequency accuracy and high frequency stability whereas at the receiving side, narrow-banded amplifiers which e.g. are provided with crystal filters and which are tuned to the signal frequency or the signal frequencies, may be provided.

The invention has a multiplicity of advantageous applications.

For example, tachycardiac rhythm disturbances so far at first are treated with drugs. On further progress of the disease, antibradycardiac stimulation by means of a sequential pacemaker of the type known from German unexamined published patent application 27 01 140 may become necessary, wherein simultaneously or at a later state it may be advantageous to supplement the antibradycardiac stimulation by antitachycardiac stimulation pattern (compare e.g., European Patent Specification 0 094 758). When this too is no longer sufficient to adequately influence the syndrome and attacks of ventricular fibrillation occur, a defibrillator becomes necessary which likewise is available as an implantable device. However, when implanting the defibrillator, the sequential pacemaker again must be explanted because this pacemaker delivers atrial and ventricular stimulating pulses which, in the same manner as possibly the R-wave of the electrocardiogram, too, are detected by the defibrillator whereby the latter sees an apparent frequency duplication or frequency triplication. When the heart works correctly with e.g. 70 beats per minute, therefore, there is the risk that the defibrillator detects an apparent heartbeat rate of 140 or 210 beats per minute and undesirably delivers a defibrillation pulse. When the pacemaker is explanted, necessarily the antibradycardiac and possibly also antitachycardiac protective effect thereof no longer exists. Besides, the drug dosage must be reduced because the patient no longer is protected against a drop of the rate of the heart activity. The defibrillator will become active relatively frequently and possibly inappropriately.

Within the scope of the present invention, it is possible to transfer the intelligent decisions, particularly the detection of the requirement of a defibrillation shock, from the defibrillator to the preferably A-V sequential, programmable, microprocessor based pacemaker and to make the defibrillator only indirectly programmable via the pacemaker making use of the body bus. The pacemaker which e.g. may be designed in the manner known from European Patent Specification 0 094 758, safely detects whether the pacemaker itself stimulates or whether there is a tachycardia. When a tachycardia is detected, the pacemaker can request the shock from the defibrillator through the body bus. Therefore, if in the course of the therapy the sequential pacemaker no longer will be sufficient, this pacemaker need not be explanted. Rather the therapy can be systematically built up as a function of the respective requirements without previous implants becoming obsolete. In view of the monitoring functions included in the pacemaker, the requirement of the additional implantation of a defibrillator function can be detected at an early state. The defibrillator, which constitutes a high current application, then can be added. Simultaneously, the sequential antibradycardial stimulation, possibly assisted by drugs, reduces the fibrillation incidence when compared with a pure ventricular stimulation. The stimulation treatment of tachycardia likewise can be carried through by the pacemaker, optionally in a dual chamber manner, whereby the effectivity of detection and of the treatment is increased thereby again reducing the probability of fibrillation. Thus the defibrillator may be restrained, as far as conceivable, to its function as an emergency or backup system.

With respect to the separation of pacemaker and defibrillator, which is easily possible by making use of the body bus, it is to be taken into consideration that the pacemaker, particularly if, in a manner known per se, it is microprocessor controlled and programmable and also includes antitachycardiac algorithms, constitutes a complex and therefore relatively expensive device which, however, merely has a low current consumption and therefore has a very long duration even if the housing volume, as desired, is small. Besides, the pacemaker may be implanted at many different body sites as a function of appropriateness. Different therefrom, a defibrillator has a high energy consumption and, if it was only in view of its storage capacitors, a large volume. It can be implanted at a few body sites only, and in view of its high energy drain, has a relatively short lifetime.

Moreover, recent clinical studies of patients implanted with AICD devices indicate that in a large number of such patients, the defibrillation shock is delivered quite infrequently, i.e. two to four times a year. Despite the infrequent delivery of the shocks, the AICD units need to be replaced within two years due to the deterioration of the batteries. The system of the present invention contemplates the possibility of replacing a large volume, large capacity defibrillator with a small volume low capacity (in other words, a limited number of shocks) in those patients where experience has shown that the patient only infrequently requires a defibrillation shock. It can be expected that in even those patient populations, the frequency of required defibrillation shocks will be diminished by the efficacy of antitachycardia pacing therapies delivered by the separate pacemaker unit.

Thus the present invention contemplates the provision of a staged therapy to the patient first involving the implantation of an intelligent pacemaker in the patient and then, if necessary, the additional implantation of a defibrillator having a shock delivery capacity tailored to the requirements of the patient, e.g. 10, 20, 100 shocks per year at maximum programmable output energy. Therefore, for all these reasons, normally it does not make sense to combine the pacemaker and the defibrillator in one and the same casing.

In addition, the body bus system components may include separate remote sensors for physiologic rate responsive pacing and/or detection of arrhythmias (to augment or replace the electrogram sensing employed to confirm malignant VT or VF) as well as a drug dispenser. The drug may be delivered into the patient's body or the patient's vascular system as is appropriate to treat the patient in a fashion which the pacemaker electronics would find appropriate. For treatment of an arrhythmia detected by the pacemaker, the drug may be delivered into the vascular system or a chamber of the heart or into the body of the patient in conformance with the appropriate delivery of the specific drug.

BRIEF DESCRIPTION OF THE DRAWINGS

In the following, the invention is explained in more detail with reference to preferred embodiments thereof:

Fig. 1 is a schematic circuit diagram of a cardiac pacemaker adapted for being programmed via the body bus;

Fig. 2 is a schematic diagram of a body bus transmitter;

Fig. 3 is a schematic circuit diagram of a body bus receiver;

Figs. 4 and 5 illustrate modified embodiments of devices designed in conformity with the present invention; and

Fig. 6 illustrates the experimental setup prepared to demonstrate body bus signal transmission.

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DESCRIPTION OF THE PREFERRED EMBODIMENTS

Fig. 1 shows an implanted microprocessor controlled, programmable cardiac pacemaker 10 comprising
 10 a central processing unit (CPU) 11, a random access memory (RAM) 12, a read-only memory (ROM or EPROM) 13, a battery 14 and an input/output unit (I/O) 15. The input/output unit includes amongst others a coder and a decoder for coding and decoding, respectively, of serial information to be exchanged between the cardiac pacemaker 10 and other implantable or external modules in the illustrated embodiment an external programming unit 42. Such programmable pacemakers and associated programming devices e.g.
 15 are known from unexamined published European Patent Application 0 011 935 and European Patent Specification 0 011 936; they, therefore, presently need no further explanation.

The input/output unit 15 is connected through an input or sensing amplifier 18 and an output amplifier 19 to the atrial electrode 20 of a pacemaker lead 21; besides it is connected through an input or sensing amplifier 22 and an output amplifier 23 to a ventricular electrode 24 of the pacemaker lead 21. A body bus
 20 receiver 26 is connected to a further input of the input/output unit 15, whereas an additional output of the input/output unit is connected to a body bus transmitter 27. The input of the body bus receiver 26 is connected to the ventricular electrode 24 and to an indifferent electrode 28 which preferably is defined by the casing of the pacemaker 10. The ventricular electrode 24 and the indifferent electrode 28 furthermore are connected to the output of the body bus transmitter 27. The ventricular electrode 24 and the indifferent
 25 electrode 28 form a transmitting and receiving dipole for the pacemaker 10. However, the atrial electrode 20 and the indifferent electrode 28 likewise can be used to define the transmitting and receiving dipole of the pacemaker 10. The heart is indicated at 29. The programming signal processor 16 is connected via an input/output unit 32 to a body bus receiver 34 and to a body bus transmitter. Inputs 36, 37 of the body bus receiver 34 and outputs 38, 39 of the body bus transmitter 35 are connected to external skin electrodes 40
 30 and 41, respectively, which are put around the wrist joints of the patient. The unit 16, together with units 32 to 35, forms an external programming device 42 having a transmitting and receiving dipole defined by electrodes 40 and 41.

The body bus transmitters 27, 35 may be designed in the manner illustrated in the schematic circuit diagram of Fig. 2. The transmitter includes an oscillator 43, preferably a crystal oscillator, which generates a
 35 preferably sinusoidal carrier signal having a fixed predetermined frequency in the medium frequency range extending from 10 kHz to 100 kHz. The oscillator 43 is keyed, in conformity with an A1-modulation, by a serial modulation signal 45 supplied to an input 44. The oscillator correspondingly supplies at its output a modulated medium frequency carrier signal 46 consisting of groups of each a plurality of carrier oscillations. The modulated carrier signal is supplied to the input of an output unit 47 which includes a transistor 48
 40 which delivers across an output resistor 49 an amplified modulated carrier signal having an amplitude of preferably 50 to 500 millivolts, e.g. about 200 millivolts.

A design suitable for the body bus receivers 26 and 34 schematically is illustrated in Fig. 3. The receiver, at the input side thereof, includes a preamplifier 50, e.g. an amplifier comprising an octocoupler. Preamplifier 50 is followed by a high-Q filter 51, preferably a crystal filter, which is tuned to the carrier
 45 frequency of e.g. 30 kHz. Filter 51 provides a narrow passband for the carrier signal and substantially suppresses signals of all other frequencies. Filter 51 is followed by a further amplifier unit 52 and a demodulator and pulse shaping unit 53 which converts the received filtered groups of carrier signal oscillations 54 into pulses 55 of predetermined amplitude and a duration defined by the code.

Returning to Fig. 1, in order to program the implanted pacemaker, i.e. for setting or changing
 50 parameters such as the rate, the amplitude and the width of the stimulation pulses, the sensitivity of the input amplifiers 18, 22, the refractory period, the detection algorithm for detecting arrhythmias (rate, onset/acceleration, number of intervals to trigger, etc.) and the like and/or for selecting one of a plurality of possible pacemaker modes, the electrodes 40, 41 are applied at a desired site of the patient, e.g. at the wrist joints, and serially coded programming commands in the form of the modulated medium frequency
 55 carrier signal are supplied to the electrodes 40, 41 from the programming unit 42 via the input/output unit 32 and the body bus transmitter 35. The transmitter dipole defined by electrodes 40, 41 transcutaneously introduces the modulated carrier signal into the body of the patient. There the signal is propagated in the ion medium of the intra and extracellular body liquids. In this manner, the modulated carrier signal is

transmitted by electrolytic-galvanic coupling to the receiving dipole defined by the ventricular electrode 24 and the indifferent electrode 28 of the pacemaker 10.

The modulated carrier signal then is amplified, filtered, demodulated and shaped in the body bus receiver 26 and is decoded via input/output unit 15 for further processing. In a corresponding manner the programming device 42 can request from pacemaker 10 information for purposes of monitoring, repeating and remote indicating or the like. This information, again in serially coded form, is communicated from the input/output unit 15 to the body bus transmitter 27 where it modulates a medium frequency carrier signal. The modulated carrier signal is applied by the transmitting dipole defined by electrodes 24, 28 to the ion medium of the body, is propagated there and transcutaneously reaches the electrodes 40 and 41 of the programming device 42 which electrodes now act as a receiving dipole. The modulated medium frequency signal is filtered out in a narrow band mode, is amplified, demodulated and shaped and finally is processed via decoding in input/output unit 32 for being applied to the signal processor unit 16 for decoding, storage and display.

Whereas the transmitters and receivers of Figs. 2 and 3 are designed for an A1-modulation, other modulation modes, particularly a pulse code modulation with shifting between a pair of carrier signal frequencies within the frequency range from 10 kHz to 100 kHz (so-called FSK-modulation) likewise can be used for the body bus receivers 26, 34 and the body bus transmitters 27, 35.

The arrangement of Fig. 1, even still afterwards, easily can be further expanded, e.g. by implantation of a defibrillator 58, as schematically illustrated in Fig. 4. The defibrillator 58 comprises a defibrillator output unit 60 adapted to be charged from a battery 59, the output side of unit 60 being connected to implanted defibrillator electrodes 61 and 62. The defibrillator output unit 60, at the input side thereof, is controlled through a body bus receiver 63 and a decoder 64 connected to the output of the latter. The inputs of the body bus receiver 63, which e.g. is designed in conformity with Fig. 3, likewise are connected to the defibrillator electrodes 61, 62 which simultaneously function as receiving dipole of the body bus. The defibrillator 58 together with its associated battery 59 is housed within its own casing, and it can be implanted at a suitable site remote from the pacemaker 10. Defibrillator 58 is controlled by pacemaker 10 which, for this purpose, is provided in a manner known per se (e.g. in conformity with U.S. Patent 4,548,209 and European Patent Specification 0 094 758) with tachycardia and/or fibrillation detection means and, if desired, likewise with means for providing antitachycardiac pacing stimulation pattern, e.g. overdrive, burst or ramp stimulation as is known in the art. In this connection, also means for indirectly programming the defibrillator through the pacemaker 10 and the body bus may be provided. The body bus permits one to intelligently employ the defibrillator 58 which itself does not comprise means for sensing and for making decisions. For example, provisions can be made by a corresponding software design of the microprocessor controlled pacemaker 10 that in case of ventricular tachycardia which cannot be interrupted by means of the pacemaker 10 at first a cardioversion attempt with low energy is caused, whereas in the case of the occurrence of ventricular fibrillation, immediately high energy defibrillation is effected by the defibrillator 58 which is correspondingly controlled by pacemaker 10.

Instead of programming pacemaker 10 by the programming device 42 connected to the skin electrodes, or in addition thereto, programming of pacemaker 10, in conformity with Fig. 4, likewise can be effected through the telephone circuit by means of a simple auxiliary device in form of a modem 66. Modem 66 includes a body bus receiver 68 and a body bus transmitter 69 which, in turn, are connected to external skin electrodes 70 and 71. Modem 66 e.g. can be designed as a modified telephone receiver having a firsthand electrode 70 at the receiver and a separate second wrist joint electrode 71. By a corresponding software design, pacemaker 10 at first can test, with the aid of test signals, the data transport rate of the used telephone network to subsequently automatically adjust the body bus transmitter 69 to the data rate adapted to be communicated. The surface ECG can be directly transmitted to the skin electrodes 70, 71. Selectively, however, it is likewise possible to make sure that all data are communicated through the body bus and that, therefore, the intracardiac ECG is telemetered. Body bus data can be derived through electrodes 70 and 71 for further purposes, e.g. all data which anyway occur in pacemaker 10 can be communicated through the telephone circuit. Data monitoring and keeping of data archives likewise is possible. Thus, in view of the fact that the medium frequency range is used, a tape recorder 72 can be connected to the skin electrodes 40, 41 or 70, 71 in order to record the body bus signals which subsequently can be centrally evaluated by a processor or computer.

Fig. 5 illustrates a further embodiment in which the defibrillator 58, too, bidirectionally receives and delivers data. For this purpose, a body bus transmitter 74 is provided in addition to the body bus receiver 63. Transmitter 74 and receiver 63 are connected to the defibrillator output unit 60 through an input/output unit 75 which provides for the necessary coding and decoding of the signals. Such a design allows more complicated software structures of the defibrillation protocol. For example, the pacemaker 10, in case of an

impending fibrillation, as a precaution, can request the defibrillator 58 to make available a shock which is not delivered to the body until the defibrillator 58 informs the pacemaker that the shock energy is ready. The pacemaker, in response to further monitoring of the heart activity, can decide whether or not the shock is to be delivered to the heart. When the shock, made ready as a precaution, is not required, the pacemaker 10 can deliver a corresponding command to the defibrillator 58, which command causes that the storage capacitor of the defibrillator is slowly discharged or that the energy stored in the storage capacitor is returned through a converter into the defibrillator battery 59, which in this case is rechargeable, in order to save energy. It is also possible that the pacemaker 10 applies possibly dangerous antitachycardiac stimulation modes not before it has made sure through the body bus that in case of an emergency the shock immediately will be available.

Fig. 5 further schematically illustrates an implantable drug delivery device 77 including a battery 78, a body bus receiver 79, a decoder 80 and a drug pump 83. The casing of the device forms a first electrode 81 connected to an input of the receiver 79, whereas a further electrode 82 is connected to a second input of receiver 79. Electrode 82 together with electrode 81 forms an implanted receiving dipole. If required, pacemaker 10 can order, through the body bus, the drug delivery device 77 to deliver a bolus of a drug. Device 77, in a manner similar to defibrillator 58 of Fig. 5, likewise can be designed for a bidirectional exchange of information to allow replies to the pacemaker 10.

Fig. 5 finally illustrates a remote physiologic sensor 84 included in the body bus system, which sensor comprises a battery 85, a coder 86, a body bus transmitter 87 and a sensor and its associated circuitry. An output of the body bus transmitter 87 is connected to a first electrode 88 defined by the sensor casing, whereas a second input of the body bus transmitter 87 is connected to an auxiliary electrode 89. Electrodes 88 and 89 form a transmitting dipole of the sensor. The sensor, in a manner known per se, is adapted to sense respiration body activity or body parameters such as arterial blood pressure, temperature, pH value, pO_2 value and the like. Corresponding signals are telemetered to the pacemaker 10 through the body bus for suitably influencing the pacemaker. For example, the sensor data may be used to confirm the existence and nature of a bradyarrhythmia or tachyarrhythmia to influence the selection of the therapy by the pacemaker, drug dispenser or defibrillator and to influence the rate of bradyarrhythmia pacing. The sensor likewise can be designed for a bidirectional exchange of data. In this case it e.g. will be possible to let the pacemaker 10 control sensor characteristics such as the sensitivity of the sensor.

It is evident that the invention can be further modified in many different ways. For example, it is possible to at first implant an AAI pacemaker provided with body bus characteristics. If later on an AV block requires ventricular stimulation, a VVI pacemaker with body bus may be additionally, e.g. myocardially, implanted. The VVI pacemaker and the AAI pacemaker, by exchanging information therebetween, can cooperate to provide for a DDD function.

A further possible application is the implantation of a pacemaker having dp/dt functions for controlling pacing rate as a function of blood pressure rate of change. In such a case, information for delivering from a simultaneously implanted drug delivery device a drug influencing the blood pressure can be transmitted through the body bus. Thereby a "closed loop" system for blood pressure control is realized.

It is apparent that in each case suitable protocols for the data transmission, for securing priorities, for providing for redundancy and the like, are to be used.

The body bus receivers likewise, in a manner known per se, may be provided with an automatic gain control (AGC).

An experimental setup prepared by the inventor to test the practicality of the body bus communication system proposed above is illustrated in Fig. 6 and comprises a physiologic saline test tank 100, two personal computers 102 and 104, a pacing lead 106 having a pair of distal electrodes 108, 110 located within the saline solution, a pair of plate electrodes 112, 114 and transmitting and receiving interconnecting circuitry. The transmitting computer 102 is coupled to the proximal terminals of the pacing lead 106 by the crystal oscillator 43, 47 corresponding to the transmitter circuit of Fig. 2 and a further optocoupler 116. Similarly, the plate electrodes 112 and 114 are coupled to the two inputs of an optocoupler and preamplifier 50, the output of which is coupled to the pulse former circuitry 51, 52, 53 which collectively correspond to the receiver circuit of Fig. 3. The output signal of the pulse former 51, 52, 53 is applied to the second personal computer 104.

The plate electrodes 112 and 114 were prepared from copper plates each having a surface of approximately 64cm^2 to electrically imitate one type of implantable defibrillator leads. The electrodes 112, 114 are placed apart a distance approximating the distance that defibrillating plate electrodes are normally spaced across the heart in actual implantations in patients. The standard endocardial bipolar pacing lead 106 is placed so that its bipolar electrodes 108, 110 are between the plate electrodes 112, 114 to approximate the location within a patient's heart. The tank 100 is filled with physiological saline solution.

The experiments were conducted to test the hypothesis that useful information could be transmitted in both directions through the conducting medium between the pacing electrodes 108, 110 and the defibrillation electrodes 112, 114.

With the 8032 based Commodore personal computer, text was entered by its keyboard which is converted into the corresponding ASCII-NR. code which is written as an 8-bit byte into a memory location. This byte is then converted into a serial train of bit pulses preceded by a leader pulse and is emitted from its cassette port so as to gate the output of the signal generator 43, 47 at 30 kHz. With an appropriate level (200 mV) these 30 kHz burst pulses are fed through the optocoupler 116 to a Medtronic bipolar Model 6901 lead 106 immersed in the physiologic saline solution. The signals are shown illustrated at points A and B in Fig. 6, the leader illustrated as the initial wide burst signal. Pulse width modulation was employed to encode the stream of bits emitted by the electrodes 108, 110 into the saline solution.

The signals emitted from the bipolar pacing electrodes 108, 110 travel through the saline solution and are picked up by the defibrillator electrodes 112, 114 and applied to the input terminals of the optocoupler in preamplifier 50. The signal level at the input terminals of the optocoupler amplifier 50 is approximately 3 mV. After filtering and amplification by the optocoupler preamplifier 50 and pulse former 51, 52, 53, the lower edge envelope curve is reconstructed so that at this stage, the serial 8 bit pulse train with its leader can be applied to an input port or user port of a second 8032 Commodore personal computer. After serial to parallel conversion, the received code is displayed on the computer screen.

During testing, the removal of the pacing lead 106 from the saline solution during transmission of the code between the transmitting computer 102 and receiving computer 104 interrupted and terminated the transmission. Thus the transmission is obtained by the bulk conductivity of the saline solution. Moreover, by reversing the electrode connections, information could just as easily be transferred from the defibrillator plate electrodes as the transmitting electrodes to the pacing electrodes 108, 110. Various experiments were conducted with the orientation of the electrodes 108, 110 to the electrodes 112 and 114 wherein it was found that the only orientation that became insufficient was when the transmitting dipole provided by the pacing electrodes 108, 110 was directly perpendicular to the receiving dipole provided by the electrodes 112, 114 (or conversely). With conformal defibrillation electrodes 112, 114 and the usual orientation of a bipolar pacing lead axially within the heart's right ventricle, it is unlikely that this insufficient orientation would be encountered in practice.

A second bipolar electrode was connected to the output and can of a Medtronic Model 8423 VVI pacemaker which was also put into the bath of saline in tank 100. The pacemaker could not be inhibited by the high frequency 30 kHz bursts being delivered through the saline medium. This test confirmed the proposition that the 30 kHz signal at the 200 mV amplitude did not mimic signals normally sensed by a pacemaker and thereby interfere with its normal operation. The waveform used, even switched at rates at about 80 bpm, would not inhibit a standard VVI pacemaker.

In tests conducted with this experimental setup, it was determined that the burst pulse modulation with a carrier in the range of 30 kHz enabled the propagation of ASCII code safely, easily and rapidly through the conductive medium of the test tank 100. The frequency and voltage related current levels employed allow for the use of already implanted heart stimulation leads without the need of synchronization into the refractory periods of the pulse generators. Since there are no side bands, extremely narrow pass amplification of the received signals would make electrical noise suppression very simple. The baud rate can exceed 400 bauds. Since the transmission speed is higher than any imaginable intracorporeal need, a high degree of safety can be achieved by redundant transmission and other forms of data encryption.

A computer listing actually used to transmit the statement "the quick brown fox jumps over the lazy dog" between the transmitting and the receiving personal computers is attached hereto as follows:

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START OF TRANSMITTER (BASIC)

```
100 rem name of program: 12b transmit.  
105 rem purpose: transmitting ascii code for bodybus.  
110 rem principle: parallel to serial conversion ('lsr')  
115 rem                and keying of a 30 kHz oscillator thru  
120 rem                cassette port #2 of a commodore  
10                computer.  
125 rem                the oscillator output (bursts, 30 kHz,  
130 rem                200 mV) is conducted into .9% saline  
15 135 rem                by a Medtronic 6901 bipolar lead.  
140 if peek (19999)<>17then poke 19999,17:load"12m  
    transmit",8,1  
145 poke 20006,12:poke20029,3:poke20037,6:poke20093,3:rem  
20    increments in lms  
150 sys63739:poke59456,227:rem initializing cassette port  
    #2 for transmission
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155 y$="_____The quick brown fox jumps over the lazy dog
      1 2 3 4 5 6 7 8 9 0"
5  160 for a=1 to 68: b$=mid$(y$,a,1): gosub 185: next a: print
    165 b=13: gosub 190
    170 print "More code entered by keyboard.": print
    175 get b$: lfb$="" then 175: rem get input from keyboard
10 180 gosub 185: goto 175
    185 b=asc(b$)
    190 print chr$(b);: poke 20003,b: sys 20004: return: rem transmit
15   ascii-#
    END OF TRANSMITTER (BASIC)

```

```

20  START OF TRANSMITTER (ASSEMBLY 6502)
    20000 nop
    20001 nop
    20002 nop
25  20003 brk
    20004 sei
    20005 lda     12
30  20007 stam 20055
    20010 jsr 20054
    20013 jsr 20092
    20016 ldx     8
35  20018 ldam 20003
    20021 clc
    20022 lsr
40  20023 stam 20003
    20026 bcs 20036
    20028 lda     3
45  20030 stam 20055
    20033 jmp 20041
    20036 lda     6
    20038 stam 20055
50  20041 jsr 20054
    20044 jsr 20092
    20047 dex
55  20048 bne 20018

```

```
20050 cli
5 20051 rts
20052 brk
20053 brk
20054 lda      3
10 20056 stam 20052
20059 lda      243
20061 stam 59456
15 20064 lda      75
20066 stam 20053
20069 decm 20053
20 20072 nop
20073 nop
20074 bne 20069
20076 decm 20052
25 20079 bne 20064
20081 lda      227
20083 stam 59456
30 20086 rts
20087 nop
20088 nop
20089 nop
35 20090 brk
20091 brk
20092 lda      3
40 20094 stam 20090
20097 lda      75
20099 stam 20091
45 20102 decm 20091
20105 nop
20106 nop
20107 bne 20102
50 20109 decm 20090
20112 bne 20097
20114 rts
55 END OF TRANSMITTER (ASSEMBLY 6502)
```

START OF RECEIVER (BASIC)

```

100 rem name of program: 12b receiver
5 105 rem purpose: receive and decode ascii code for
110 rem principle: bodybus amplification, filtering,
111 rem pulse forming and decoding ('ror').
112 rem The signals (bursts, 30 kHz, .6mV) are
10 113 rem received through 2 copper plates
114 rem immersed in .9% saline, surface each
ca. 64 sq. cm.

15 115 ifpeek(19999)<>17thenpoke19999,17:load"12m
receiver",8,1
120 poke20016,8:poke20087,4:rem speed intervals in ms
125 sys20000:rem start of 12m receiver
20 130 printchr$(peek(20063));:rem print received character
on screen
135 go to 125
25 END OF RECEIVER (BASIC)

```

START OF RECEIVER (ASSEMBLY 6502)

```

30 20000 sei
20001 lda 1
20003 bitm 59471
20006 bne 20001
35 20008 jmp 20015
20011 nop
20012 nop
40 20013 brk
20014 brk
20015 lda 8
45 20017 stam 20013
20020 lda 75
20022 stam 20014
20025 lda 1
50 20027 bitm 59471
20030 bne 20045
20032 decm 20014
55 20035 bne 20025

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20037 decm 20013
20040 bne 20020
5 20042 jmp 20050
20045 cli
20046 rts
10 20047 nop
20048 nop
20049 nop
20050 lda
15 20052 bitm 59471
20055 beg 20050
20057 jmp 20067
20 20060 nop
20061 nop
20062 nop
25 20063 oram 10753
20066 brk.
20067 ldx 8
20069 lda 255
30 20071 stam 20066
20074 decm 20066
20077 bne 20074
35 20079 lda 1
20081 bitm 59471
20084 bne 20079
20086 lda 4
40 20088 stam 20064
20091 lda 57
20093 stam 20065
45 20096 lda 1
20098 bitm 59471
20101 bne 20116
20103 decm 20065
50 20106 bne 20096
20108 decm 20064
20111 bne 20091
55 20113 jmp 20127
```

```

20116 clc
5 20117 ldam 20063
20120 ror
20121 stam 20063
10 20124 jmp 20142
20127 sec
20128 ldam 20063
20131 ror
15 20132 stam 20063
20135 lda 1
20137 bitm 59471
20 20140 beg 20135
20131 dex
20143 bne 20069
25 20145 cli
20146 rts
END OF RECEIVER (ASSEMBLY 6502)

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30 From the foregoing description, it will be apparent that the body bus system of the present invention has a number of advantages, some of which have been described above and others of which are inherent in the invention. Also it will be apparent that modifications can be made to the system without departing from the teachings of the present invention. Accordingly, the scope of the invention is only to be limited as
35 necessitated by the accompanying claims.

Claims

- 40 1. In a system for monitoring a condition of a living body and/or providing one or more therapy regimens to the body comprising two or more discrete medical devices, at least one of which is implanted into the living body, the improvement for providing bidirectional exchange of information between said medical devices comprising:
means associated with at least one of said medical devices for providing a first information signal representing a condition of the device and/or the living body;
45 means for transforming said first information signal into a modulated medium frequency signal in the frequency range from 10 to 100 kHz;
means for applying said modulated medium frequency signal to the ion medium of the intra and extracellular body liquids for providing an electrolytic/galvanic coupling between said two or more medical devices whereby said signals are passed through said living body between said medical devices; and
50 means associated with at least the other of the two medical devices for receiving and demodulating said modulated medium frequency signal.
2. The system according to claim 1 wherein said medium frequency signal is modulated at 30 kHz.
3. The system according to claim 1 or 2, characterized in that a cardiac pacemaker is provided as an implantable medical device.
- 55 4. The system according to claim 3, characterized in that a defibrillator, which is separate from said cardiac pacemaker, is provided as a further implantable medical device.
5. The system according to claim 4, characterized in that both said cardiac pacemaker and said defibrillator are provided with transmitting and receiving means.

6. The system according to any one of claims 3 to 5, characterized in that in case a plurality of implantable medical devices are provided, programming and/or intelligent decision means are concentrated in said cardiac pacemaker and that other medical devices are indirectly programmable via said cardiac pacemaker.
- 5 7. The system according to claim 1, characterized in that in case a plurality of implantable medical devices are provided, programming and/or intelligent decision means are concentrated in only one of the implantable medical devices and that other medical devices are indirectly programmable via said medical device.
8. The system according to any one of the preceding claims, characterized in that a drug delivery
10 device is provided as an implantable medical device.
9. The system according to any one of the preceding claims, characterized in that a sensor for detecting a body parameter is provided as an implantable medical device.
10. The system according to any one of the preceding claims, characterized in that a controllable and/or programmable artificial organ is provided as an implantable medical device.
- 15 11. The system according to any one of the preceding claims, characterized in that a monitoring or test device is provided as an external medical device.
12. The system according to claim 11, characterized in that a modem adapted for connection to a telephone circuit is provided as an external medical device.
13. The system according to claim 11 or 12, characterized in that a data recording device is provided
20 as an external medical device.
14. The system according to any one of the preceding claims, characterized in that the medical devices are provided with means for receiving and/or transmitting of pulsecode-modulated medium frequency signals.
15. The system according to any one of the preceding claims, characterized in that the medical devices
25 are provided with means for receiving and/or transmitting A1-modulated medium frequency signals.
16. The system according to any one of claims 1 to 14, characterized in that the medical devices are provided with means for receiving and/or transmitting signals which are frequency-shifted between a pair of frequencies within the medium frequency range.
17. The system according to any one of the preceding claims, characterized in that the modulated
30 medium frequency signals have an amplitude from 50 to 500 millivolts and a frequency of 30 kHz.
18. The system according to claim 1 further comprising:
at least one digitally programmable, implantable medical device and an external medical device for digitally programming said implantable medical device wherein said implantable medical device is provided with:
a pair of spaced apart electrodes adapted to be exposed to living body tissue and fluids;
35 receiving means for receiving electrical signals across said electrodes;
decoding means for decoding said electrical signals; and
register means for storing said decoded electrical signals; and
wherein said digital programming device further comprises:
a pair of electrodes adapted to be placed against the external surface of the living body;
40 coding means for coding a desired program change into digital code; and
transmitting means responsive to the programmed digital code for modulating said digital signal and applying it to said external pair of electrodes whereby said modulated medium frequency signal in the frequency range from 10 to 100 kHz is applied through the skin and living body tissue to said implantable pair of electrodes.
- 45 19. The system according to claim 1 wherein a first body implantable medical device comprises means for providing a therapy to the living body and wherein a second medical device comprises a remotely implanted physiological body condition detecting device and further includes:
sensor means for sensing a physiological parameter in a body;
signal converting circuit means for converting signals generated by said sensor means to modulated
50 medium frequency signals in the frequency range from 10 to 100 kHz;
a first pair of spaced-apart electrodes adapted to be placed in contact with the body tissue within the living body;
transmitting means for transmitting said modulated signal to said first medical device by applying said modulated signal across said first spaced-apart implanted electrodes; and
55 wherein said first medical device further comprises:
a second pair of spaced-apart electrodes implanted within the living body in contact with body tissue; and
receiving means coupled to said second pair of electrodes for demodulating and decoding said signal transmitted from said first medical device.

20. A system for monitoring a condition of a living body and/or providing one or more therapy regimens to the body comprising two or more discrete medical devices, at least one of which is a digitally programmable, implantable medical device and the other is an external medical device for digitally programming said implantable medical device wherein said implantable medical device is provided with:
- 5 a pair of spaced-apart electrodes adapted to be exposed to living body tissue and fluids;
 - receiving means for receiving electrical signals across said electrodes;
 - decoding means for decoding said electrical signals; and
 - register means for storing said decoded electrical signals; and
 - wherein said digital programming device further comprises:
 - 10 a pair of electrodes adapted to be placed against the external surface of the living body;
 - coding means for coding a desired program change into digital code; and
 - transmitting means responsive to the programmed digital code for modulating said digital signal and applying it to said external pair of electrodes whereby said modulated, coded signal is applied through the skin and living body tissue to said implantable pair of electrodes.
21. The system according to claim 20 wherein said body implantable medical device comprises means for providing a therapy to the living body, and the system includes a further body implantable medical device comprises a remotely implanted physiological body condition detecting device further includes:
- sensor means for sensing a physiological parameter in a body;
 - signal converting circuit means for converting signals generated by said sensor means to modulated
 - 20 signals;
 - a first pair of spaced-apart electrodes adapted to be placed in contact with the body tissue within the living body;
 - transmitting means for transmitting said modulated signals to said first medical device by applying said modulated signals across said first spaced-apart implanted electrodes; and
 - 25 wherein said first implantable medical device further comprises:
 - a second pair of spaced-apart electrodes implanted within the living body in contact with body tissue; and
 - receiving means coupled to said second pair of electrodes for demodulating and decoding signal transmitted from said first medical device.
22. The system according to claim 21 wherein said first implantable medical device further comprises:
- 30 means for providing a control signal for controlling the operation of said sensor means of said further body implantable medical device;
 - means for coding said control signal;
 - transmitting means for transmitting said coded control signal to said further medical device by applying said coded control signal across said second pair of electrodes;
 - 35 wherein said further body implantable medical device further comprises receiver means coupled to said first pair of spaced-apart electrodes for receiving electrical signals appearing across said electrodes;
 - decoding means for decoding said electrical signals; and
 - register means for storing said decoded control signals, whereby the operating condition of said sensor means may be remotely controlled by said first body implantable medical device.
- 40 23. The system according to claim 22 wherein said digitally programmable, implantable medical device, said further body implantable medical device and said external medical device each respectively transmit and receive modulated medium frequency signals in the frequency range from 10 to 100 kHz.
24. The system according to claim 21 wherein said sensor means for sensing a physiological parameter in a body comprise means for sensing one or more of the body conditions including respiration, body
- 45 activity or body parameters including arterial blood pressure, rate of change of blood pressure, temperature, pH value, pO₂ value.
25. The system for providing pacing, cardioversion and defibrillation staged therapies for bradycardia, tachycardia and fibrillation comprising:
- a body implantable pacemaker comprising:
 - 50 a pacing energy pulse generator for applying pacing stimuli to a patient's heart;
 - pacing lead means bearing at least one electrode adapted to be placed in contact with or within a patient's heart and coupled to said pulse generator means for applying said pacing stimuli to the patient's heart and receiving electrical signals appearing at the tissue-electrode interface;
 - sensing means coupled to said electrode means for sensing electrical signals appearing at said electrode
 - 55 means;
 - detecting means responsive to said sensing means for detecting a bradyarrhythmia, tachyarrhythmia or ventricular fibrillation condition of the heart of the patient; and
 - control means responsive to said detecting means for instructing said pulse generator means to provide

pacing stimuli to said electrodes in response to the detection of a bradyarrhythmia or tachyarrhythmia condition and in response to the detection of a ventricular fibrillation condition provide a coded instruction signal to said pulse generator means for providing electrical signals to said electrode means; and a remotely implanted defibrillator further comprising:

- 5 defibrillation electrode means adapted to be placed in contact with a patient's heart for providing defibrillation shocks to the heart and for picking up electrical signals appearing at the electrode-tissue interface;
- defibrillation pulse generator means for providing defibrillation shocks to the heart;
- receiving means coupled to said defibrillation electrodes for demodulating and decoding said coded signal
- 10 transmitted into body tissue by said pacemaker pulse generator; and
- means responsive to a shock instruction signal decoded by said receiving means for causing said pulse generator means to provide a shock across said defibrillation electrode and to the heart.

26. The system according to claim 25 wherein:

said defibrillator further comprises:

- 15 transmitting means coupled to said defibrillation electrodes;
- coding means for coding data representing the condition of the defibrillator for providing a further coded signal to said transmitting means; and
- said pacemaker further comprises:
- receiving means for receiving said further coded data; and
- 20 said control means comprises means responsive to said further coded data for providing instructions to said defibrillator.

27. An implantable defibrillator-pacemaker system, characterized in that the defibrillator is designed to have the operation thereof controlled by the separately implanted pacemaker.

- 28. The implantable defibrillator-pacemaker system of claim 27 wherein transmitting and receiving
- 25 means are provided for effecting control signal transmission between said pacemaker and said defibrillator by coded pulse trains.

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Fig. 1

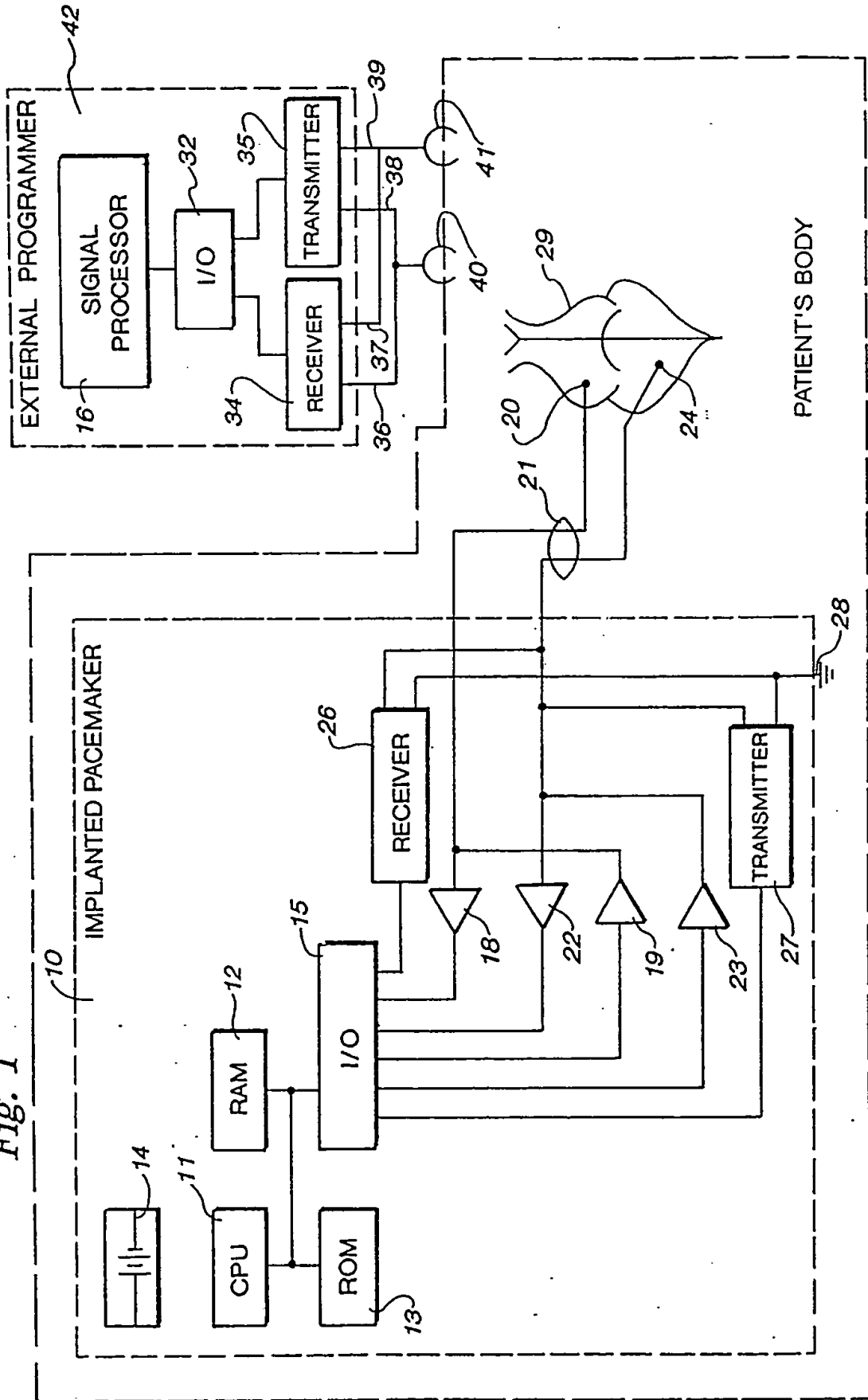


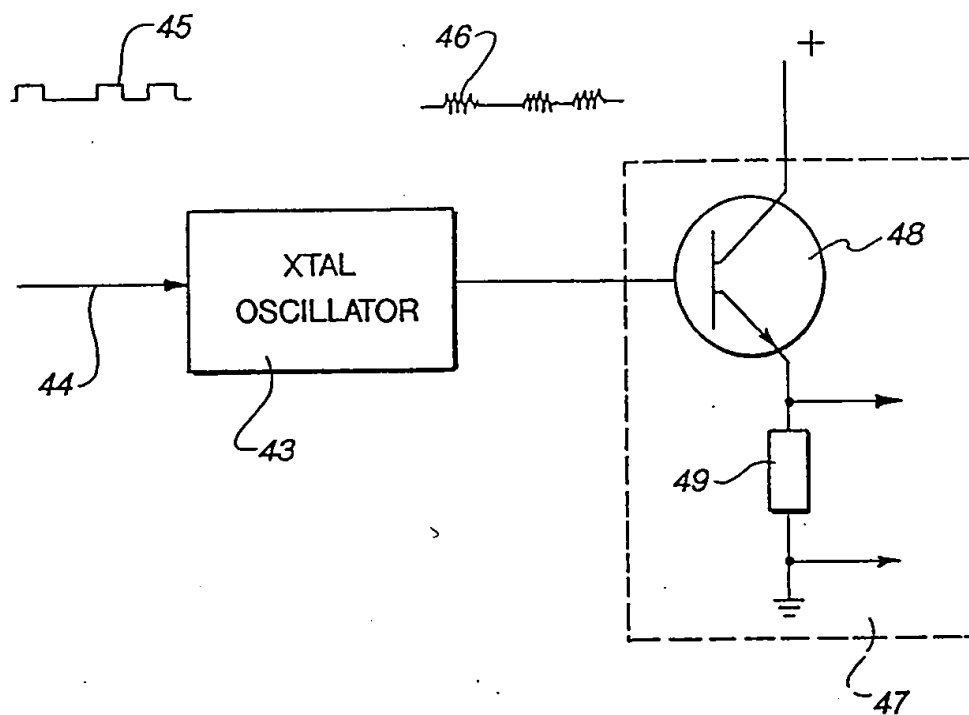
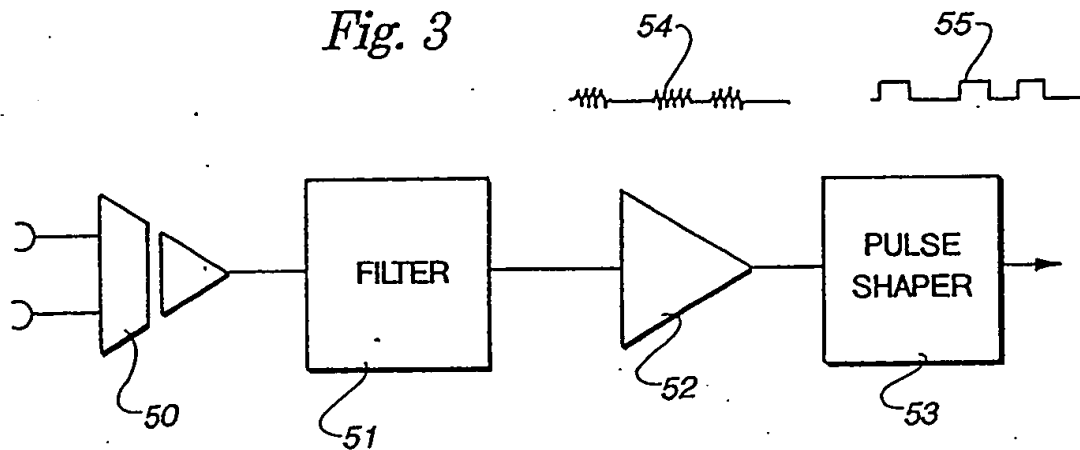
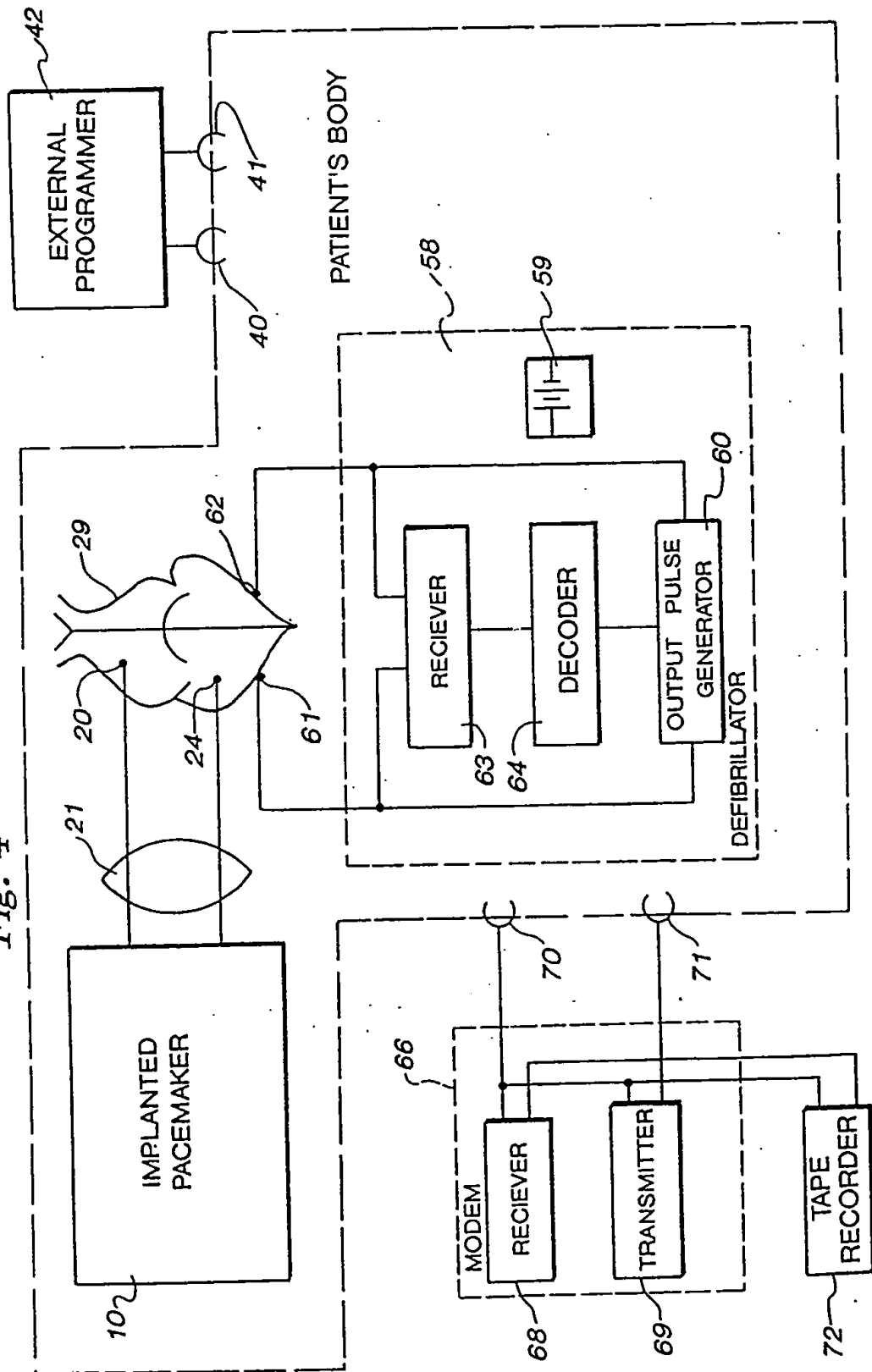
Fig. 2*Fig. 3*

Fig. 4



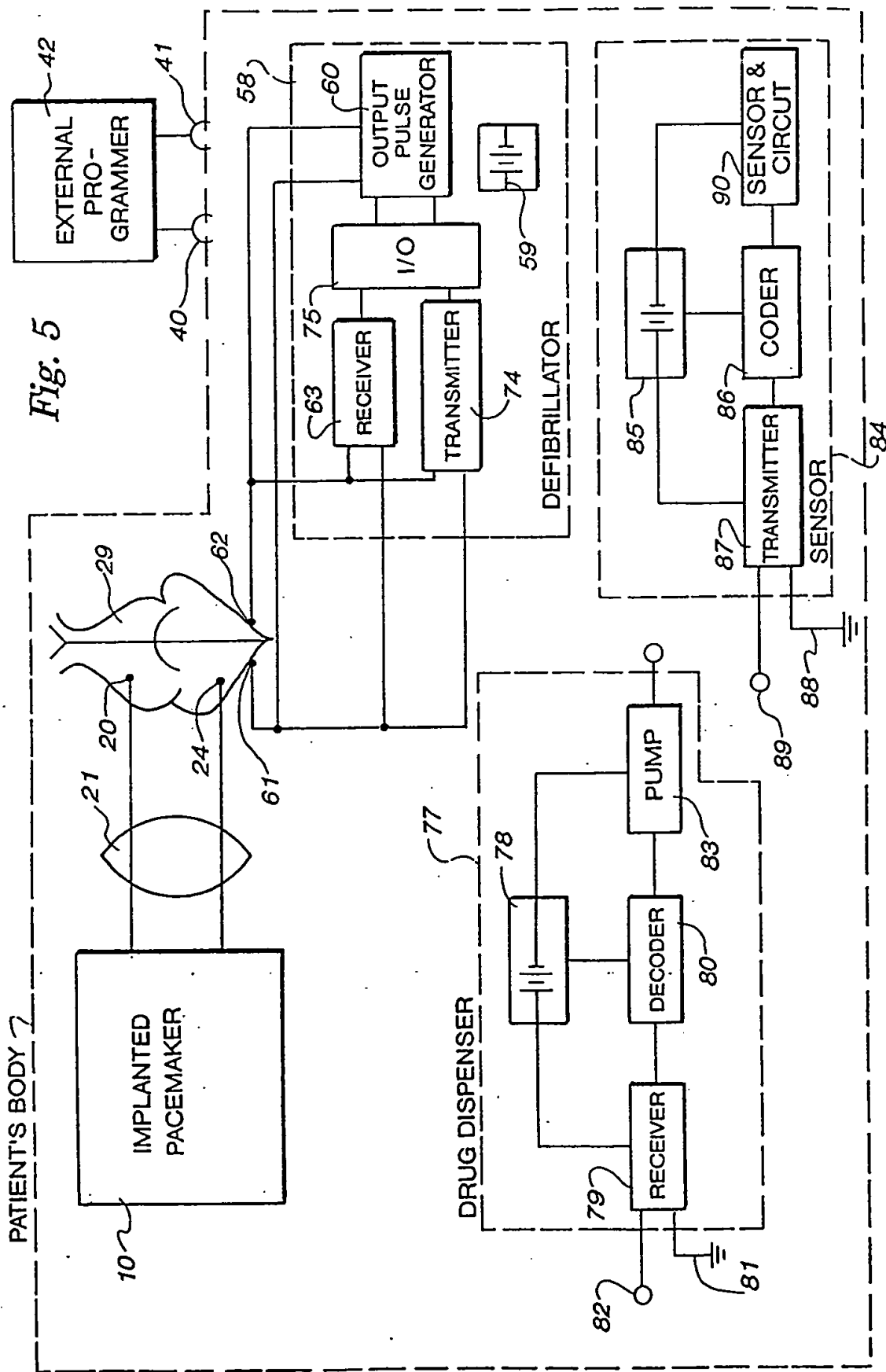
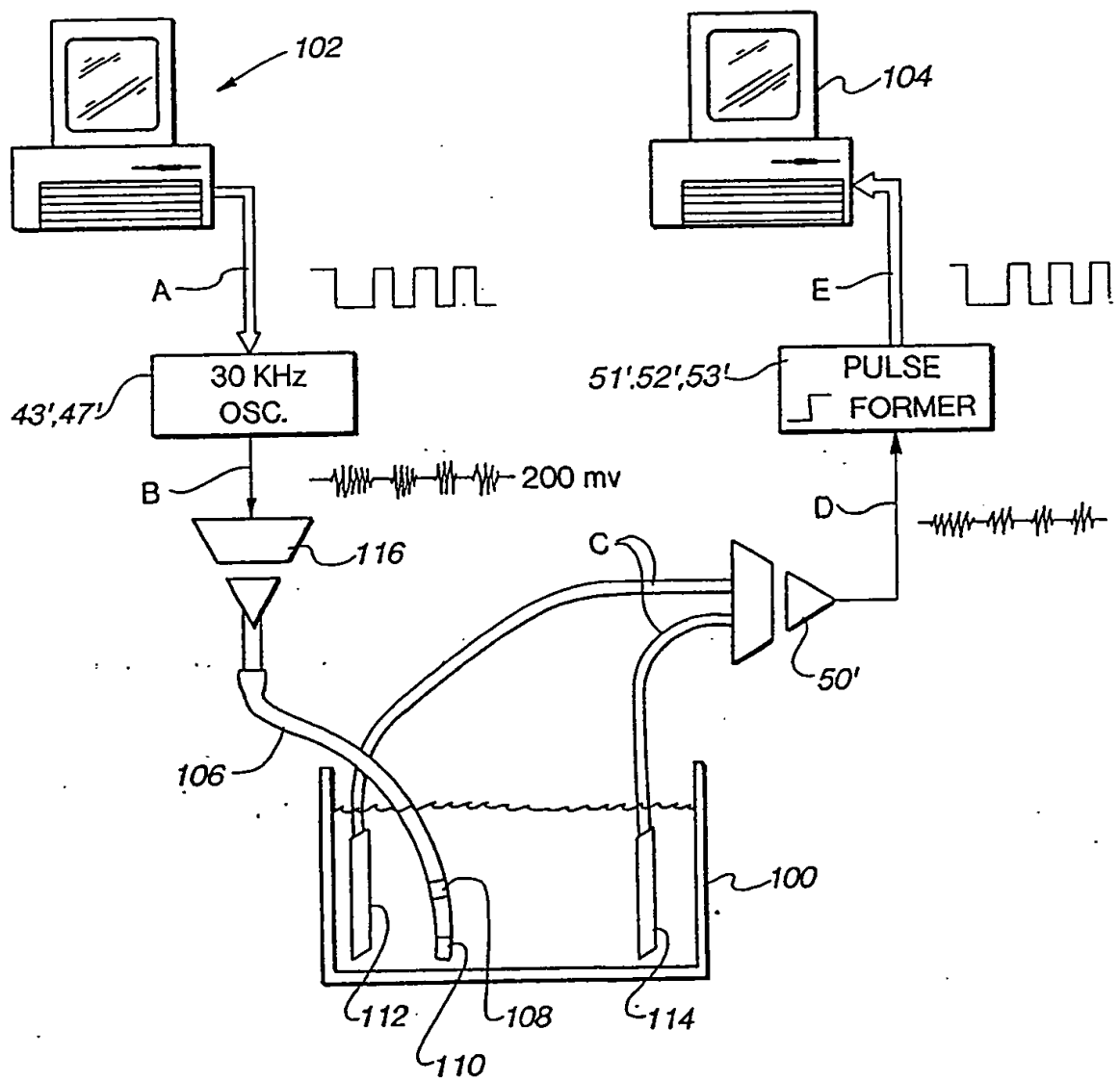


Fig. 6





DOCUMENTS CONSIDERED TO BE RELEVANT			EP 89117237.1
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int. Cl.)
X	<u>US - A - 4 313 441</u> (BUFFET) * Abstract; column 3, lines 9-13; column 4, lines 7-16, 21-26; fig. 1 * --	1, 3, 9, 11, 18-21	A 61 N 1/08 A 61 N 1/362 A 61 F 2/48 H 04 R 25/00
A	<u>US - A - 4 515 160</u> (KEIMEL) * Abstract; fig. 2, 3 * --	1, 3, 18-21	
A	<u>EP - A1 - 0 097 264</u> (SIEMENS-ELEMA) * Abstract; page 1, line 1 - page 3, line 5; fig. 1 * --	1, 3, 18-21	
A	<u>US - A - 4 153 061</u> (NEMEC) * Abstract; column 1, line 60 - column 2, line 4; fig. 1 * --	1, 18-20	
A	<u>US - A - 4 532 932</u> (BATTY) * Abstract; column 1, lines 9-40; column 2, lines 31-56; fig. 1 * --	1, 18-20	TECHNICAL FIELDS SEARCHED (Int. Cl.) A 61 N A 61 F H 04 R
A	<u>US - A - 4 690 142</u> (ROSS) * Abstract; fig. 1-3 * --	1, 18-20	
A	<u>US - A - 4 207 441</u> (RICARD) * Abstract; fig. 1 * ----	1, 18-20	
The present search report has been drawn up for all claims			
Place of search		Date of completion of the search	Examiner
VIENNA		15-01-1990	NEGWER
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document			